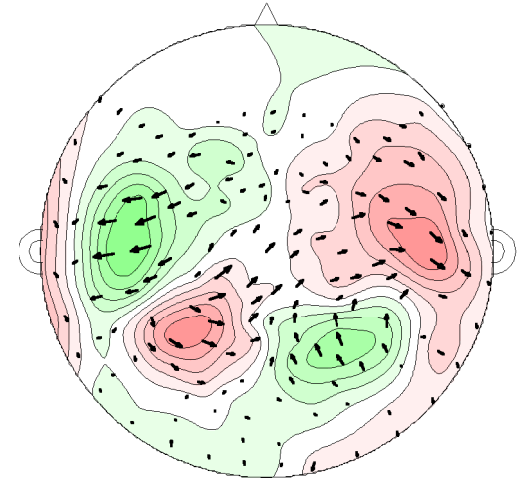


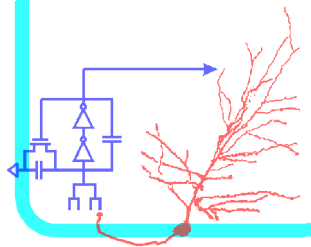
Neural Coding of Multiple Stimulus Features in Auditory Cortex



Jonathan Z. Simon

Neuroscience and Cognitive Sciences
Biology / Electrical & Computer Engineering

University of Maryland, College Park



Computational Sensorimotor Systems Laboratory

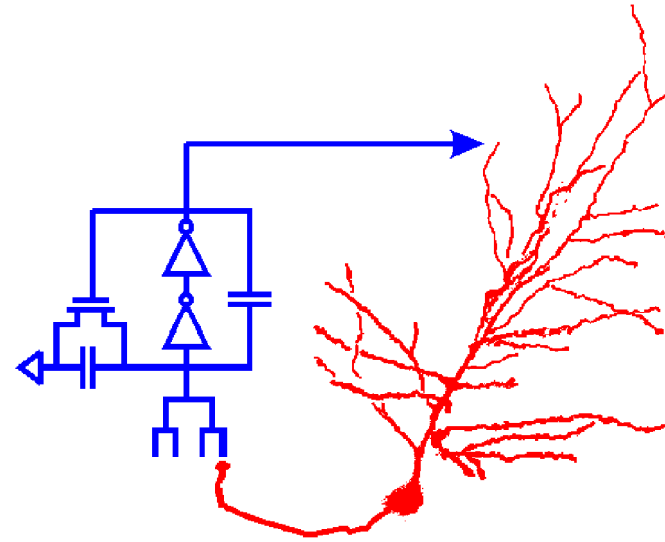
Huan Luo

Maria Chait

Juanjuan Xiang

Nayef Ahmar

Yadong Wang



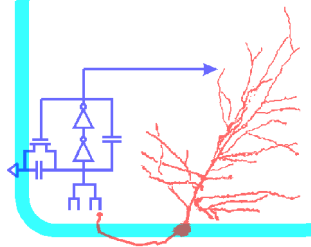
David Poeppel

Shihab Shamma

Catherine Carr

Cindy Moss

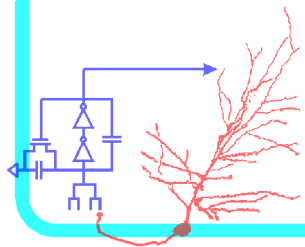
Timothy Horiuchi



Luo, H., Y. Wang, D. Poeppel & J. Z. Simon (2006), J. Neurophysiology

Introduction

- Magnetoencephalography (MEG) as a tool of Non-Invasive Auditory Physiology
- Neural Encoding of Simple Modulations
- Neural Encoding of Independent Modulation Pairs (AM & FM)



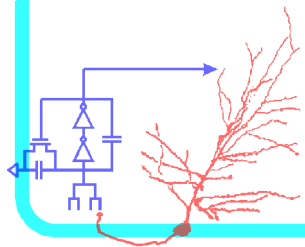
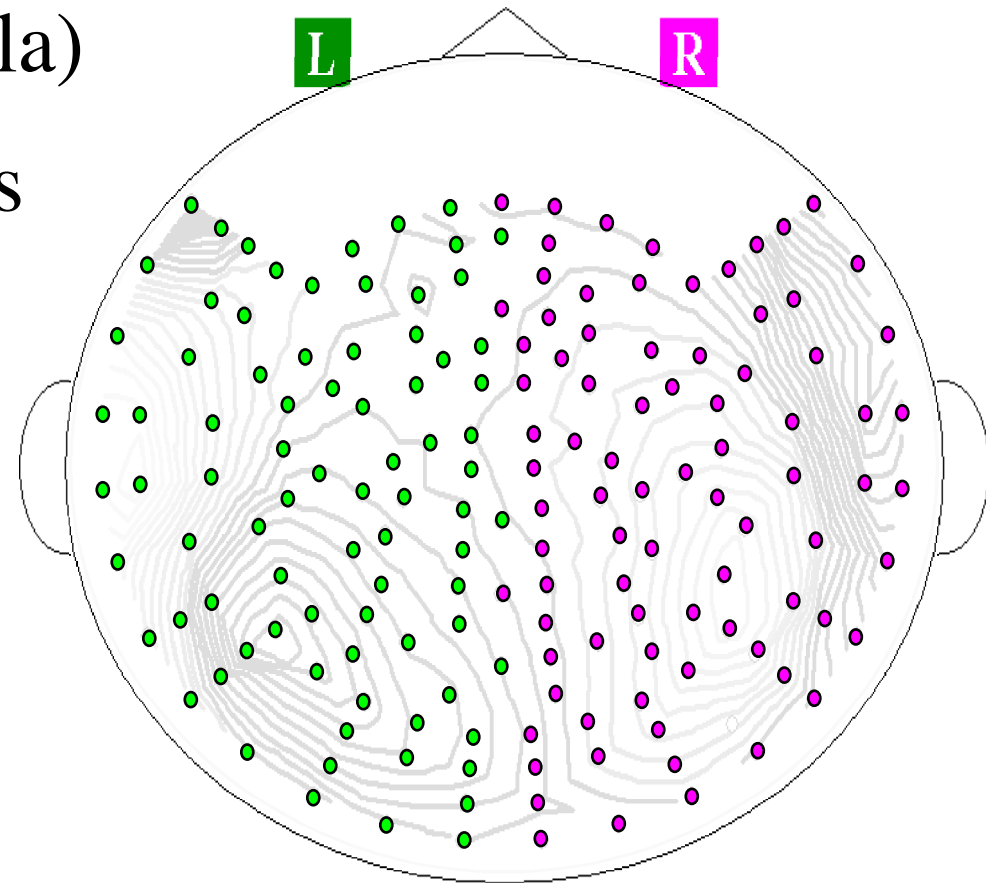
Magnetoencephalography (MEG)

- Non-invasive, Passive, Silent
- Simultaneous Whole-Head Recording (~200 sensors)
- Sensitivity

high: ~ 100 fT (10^{-13} Tesla)

low: $\sim 10^4 - \sim 10^6$ neurons

- Temporal Resolution: ~ 1 ms
- Spatial Resolution
coarse: ~ 1 cm
ambiguous



Neural Activity = Neural Current

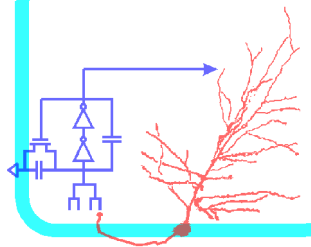
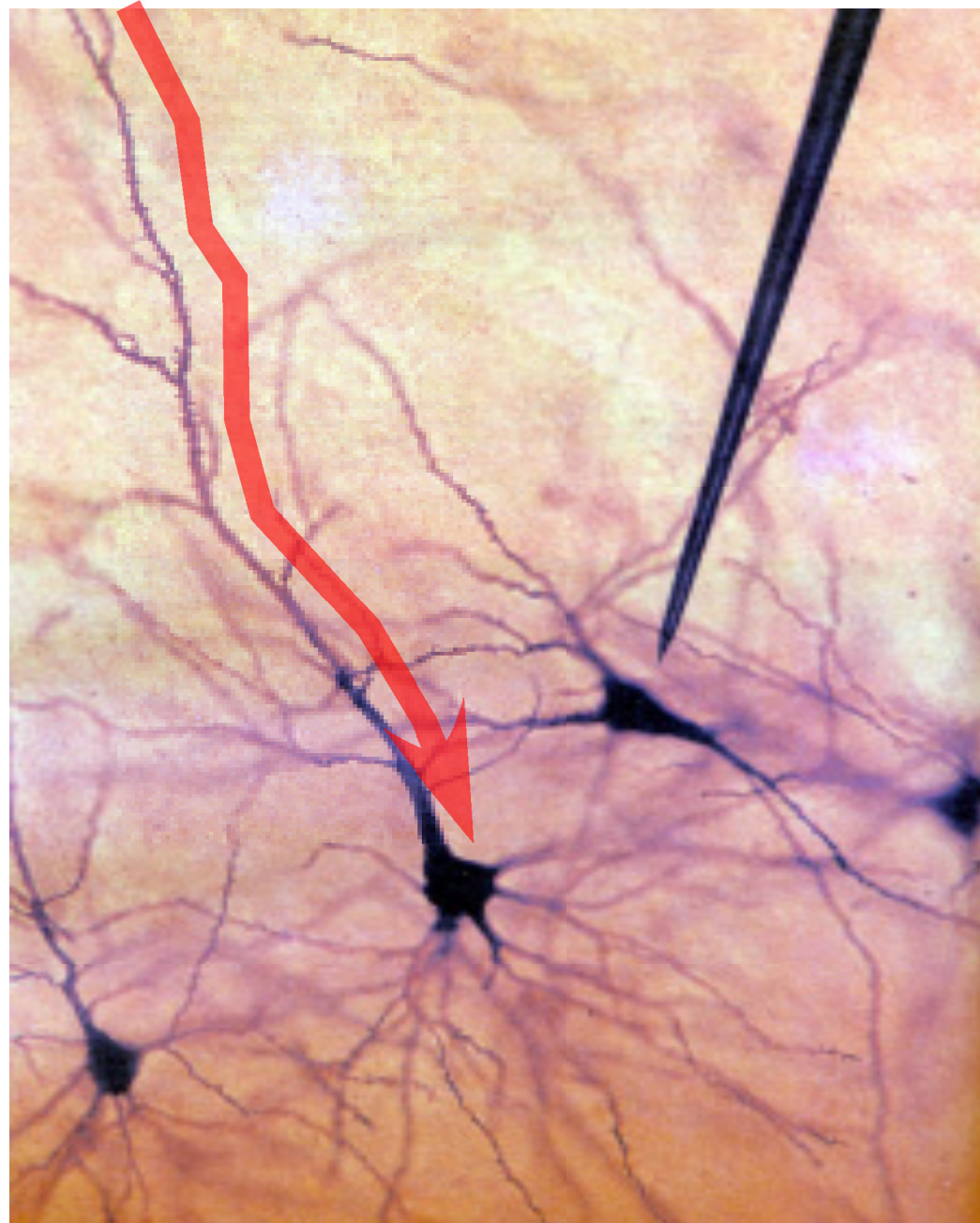
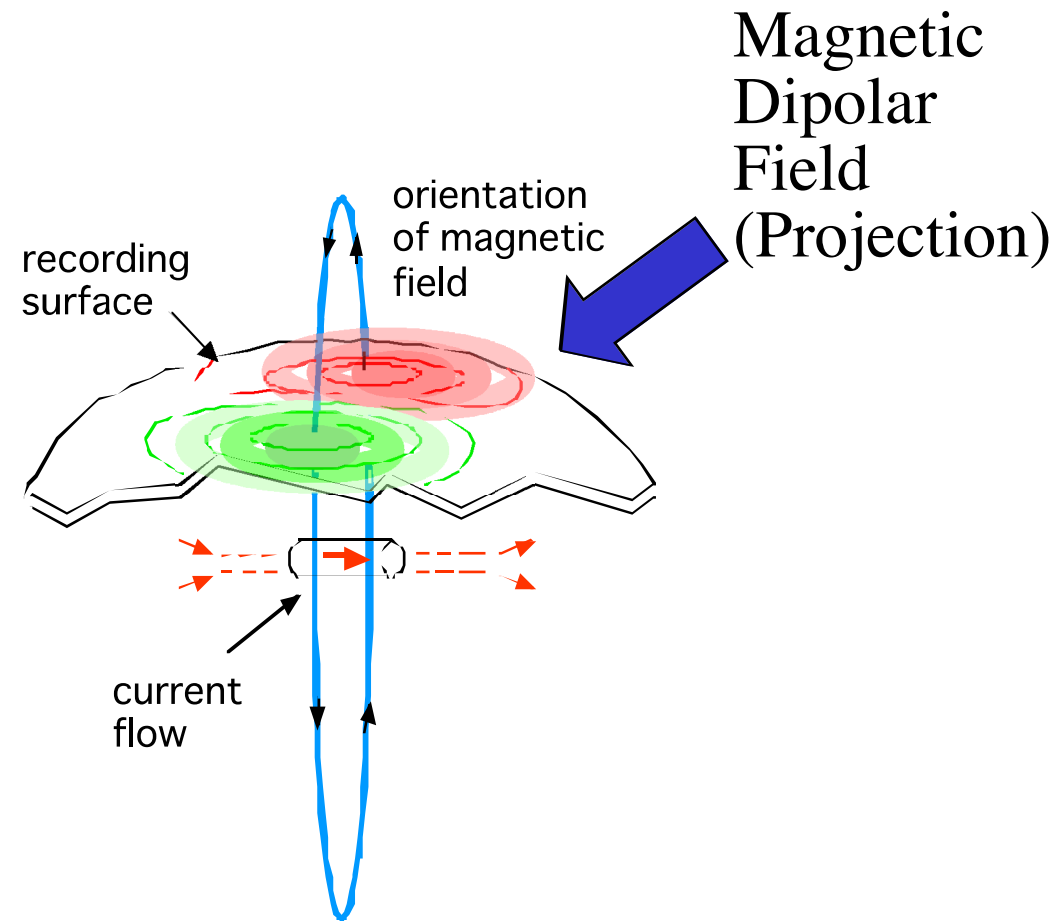
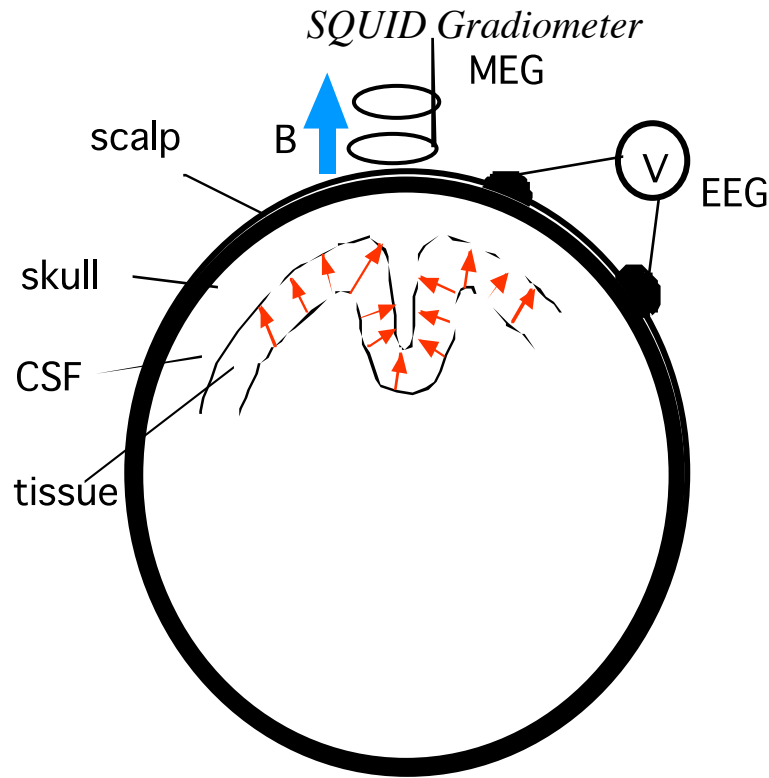


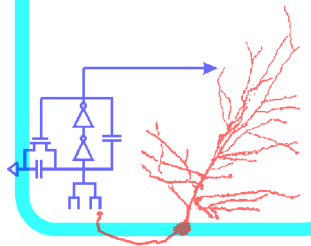
Photo by Fritz Goro

Computational Sensorimotor Systems Laboratory

MEG Magnetic Signal

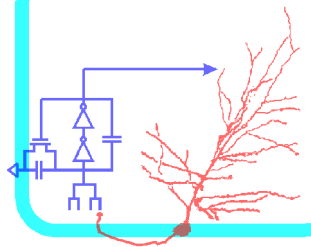
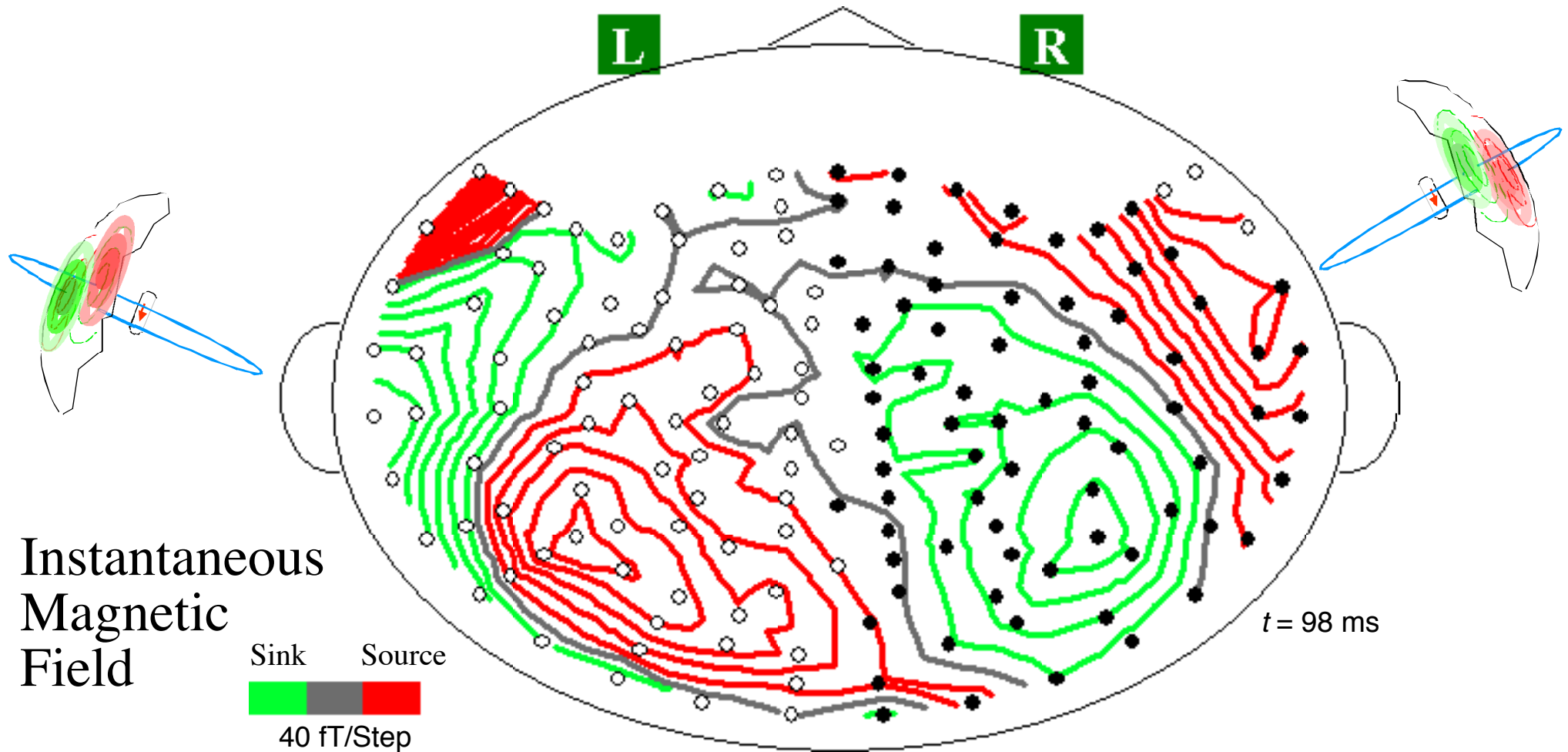


- Direct electrophysiological measurement
 - not hemodynamic
 - real-time
- No unique solution for distributed source



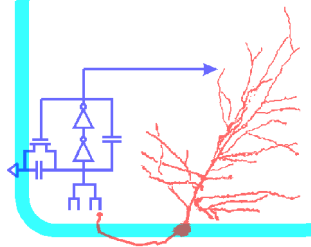
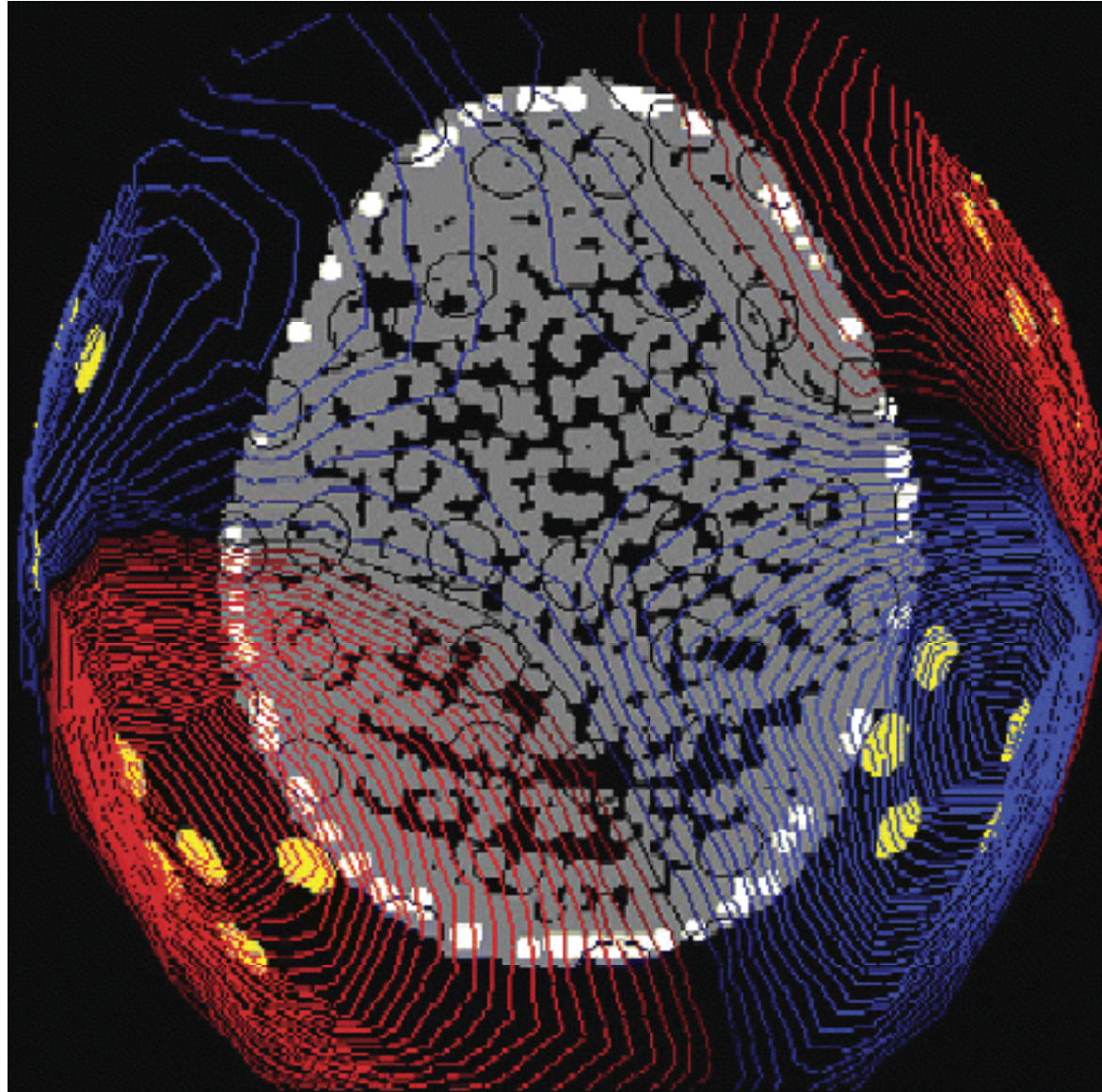
MEG Response

Flattened Isofield Contour Map



MEG Response

3-D Isofield Contour Map



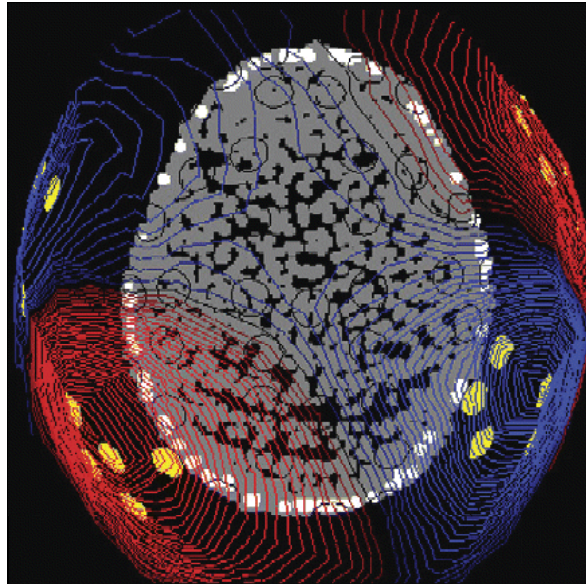
Public Relations Moment

Cerebral CORTEX

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About the Cover



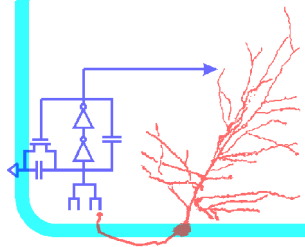
Cover Picture: Axial view of the cortically-generated magnetic field of a human listener, measured using whole-head magnetoencephalography (MEG), at a single moment in time. Isofield contours in red (respectively, blue) indicate the strength of outward (inward) magnetic flux; the digitized scalp surface is in gray. For each hemisphere, a magnetic dipole-like pattern is centered over temporal cortex, and the neural generator itself, located in planum temporale, is an inferiorly flowing neuronal electric current. The MEG channels responding most strongly (in the center of each flux area) are designated by filled yellow circles. The acoustic stimulus is a 1 kHz pure tone; time is 100 ms post onset. The image is generated with the MEG160 software (Yokogawa electric corporation, KIT, Japan). See Chait, Poeppel, and Simon, p. 835-848.

[\[Table of Contents\]](#)

Online ISSN 1460-2199 - Print ISSN 1047-3211

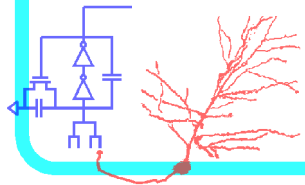
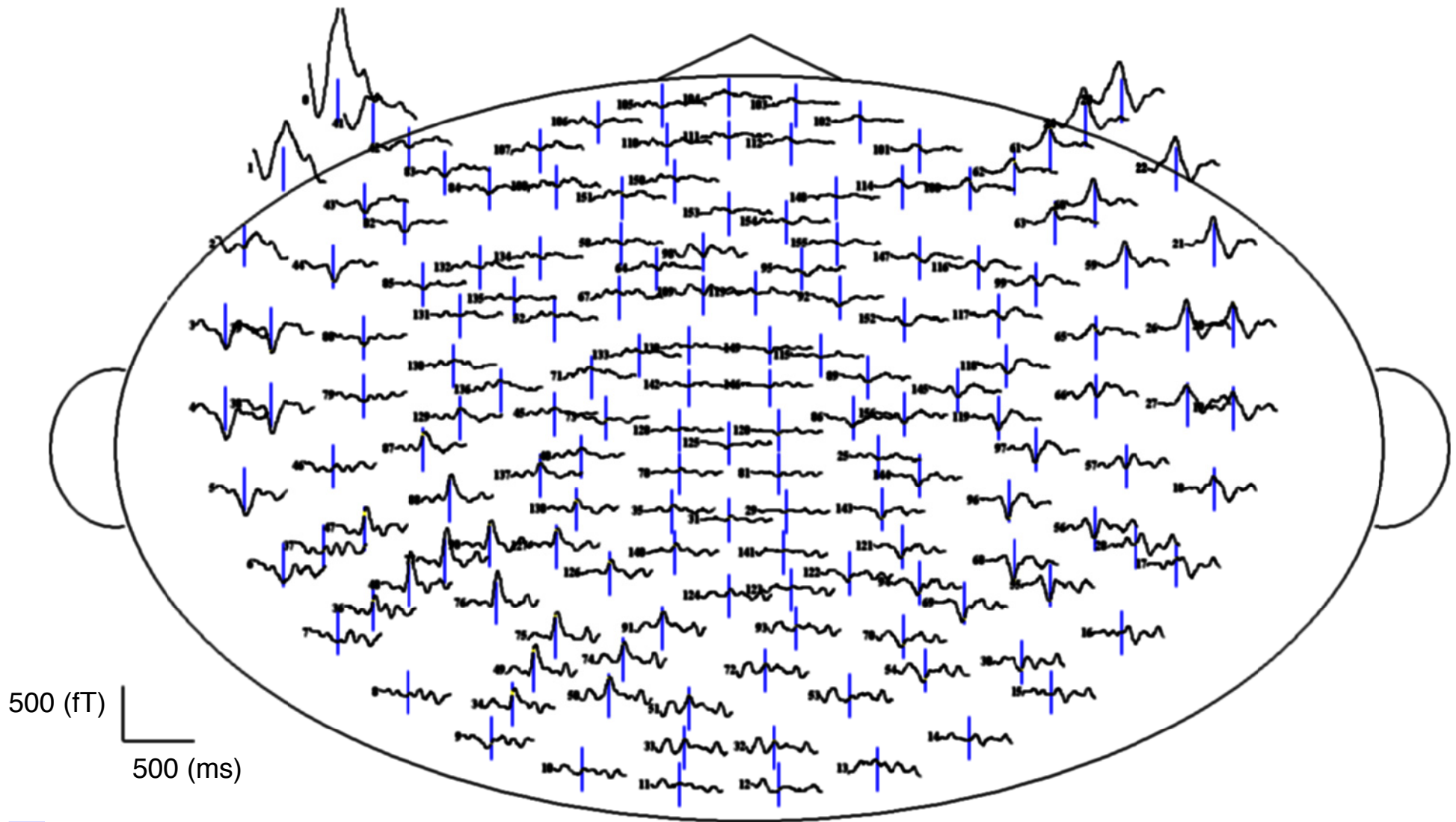
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MEG Response

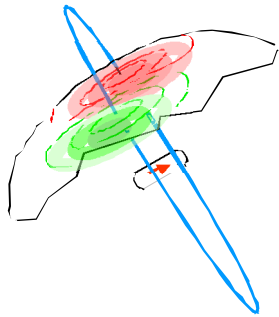
Spatial Map of Time Series



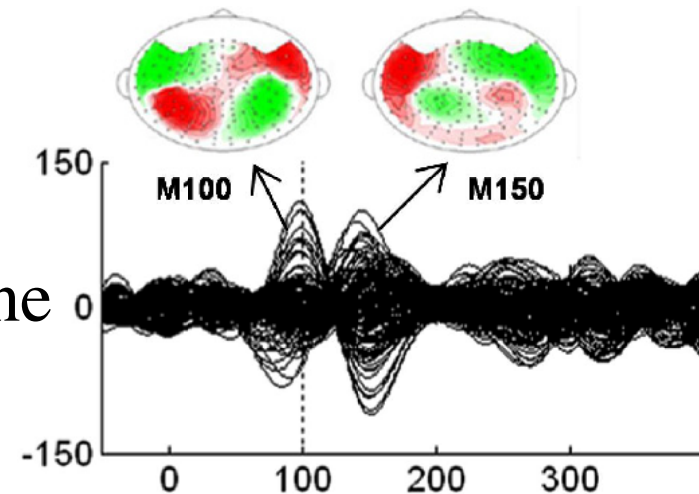
Time Course of MEG Responses

Evoked Responses

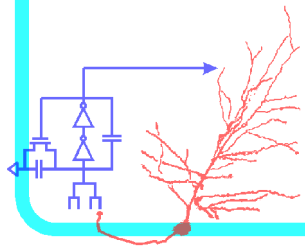
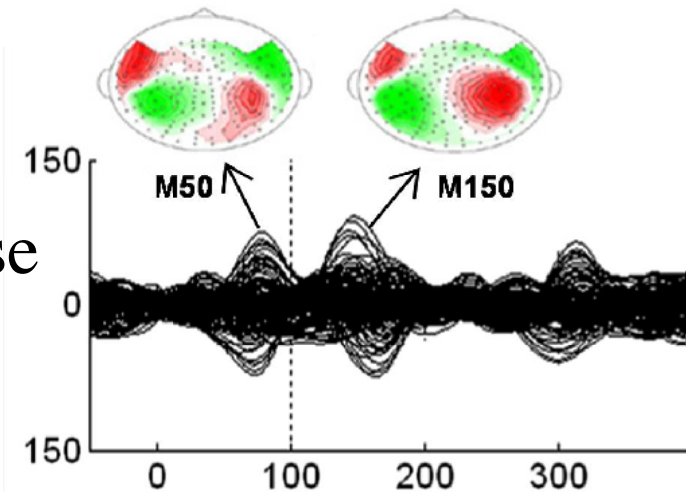
MEG Events Time-Locked
to Stimulus Event



Pure Tone

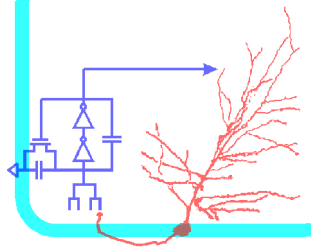


Broadband Noise



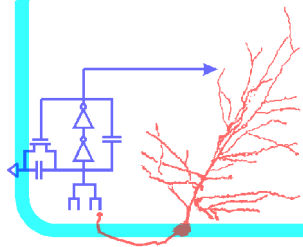
MEG as Auditory Physiology Tool

- Advantages of humans over animals
 - Subjects can be rented (by the hour)
 - Subjects can be trained in minutes
 - Better grasp of subjects perceptual space (?)
 - Access to Speech & Language processing (?)
- Advantage of Whole Head Recording
- Disadvantage of Neural Source Localization
 - Coarseness/Ambiguity in Source Location
 - Blindness to Many Kinds of Coding
- Neutral Aspects
 - Neural Source is Dendritic Current (not Spikes)
 - Humans not typical mammals (?)
 - New Technique/Immature Analysis Tools



Modulation Encoding

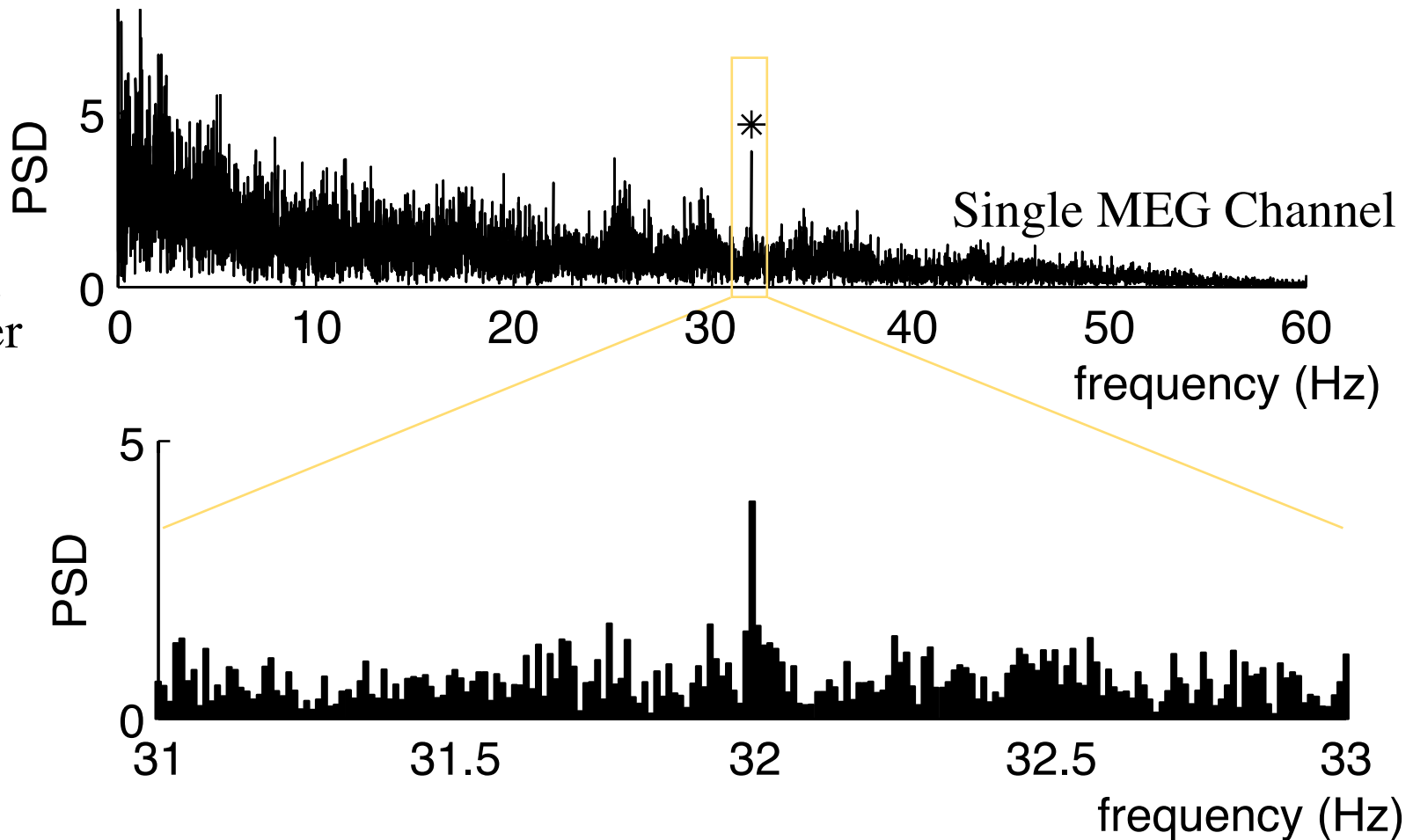
- Simple Modulations → Simple Cortical Encoding
 - Amplitude Modulation coding for slower modulations
 - Rate coding (invisible to MEG) for faster modulations
- Applies to general modulations: AM, FM, other
- Amplitude Modulation coding is easily detectable in Fourier/Spectral domain
 - Spectral Peak at Modulation Frequency



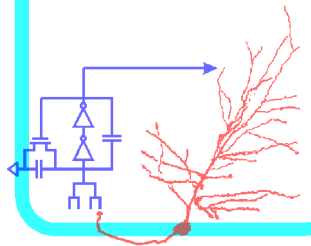
Frequency Response

Stimulus Modulated at Single Frequency $\Rightarrow$ *Steady State Response* (SSR)

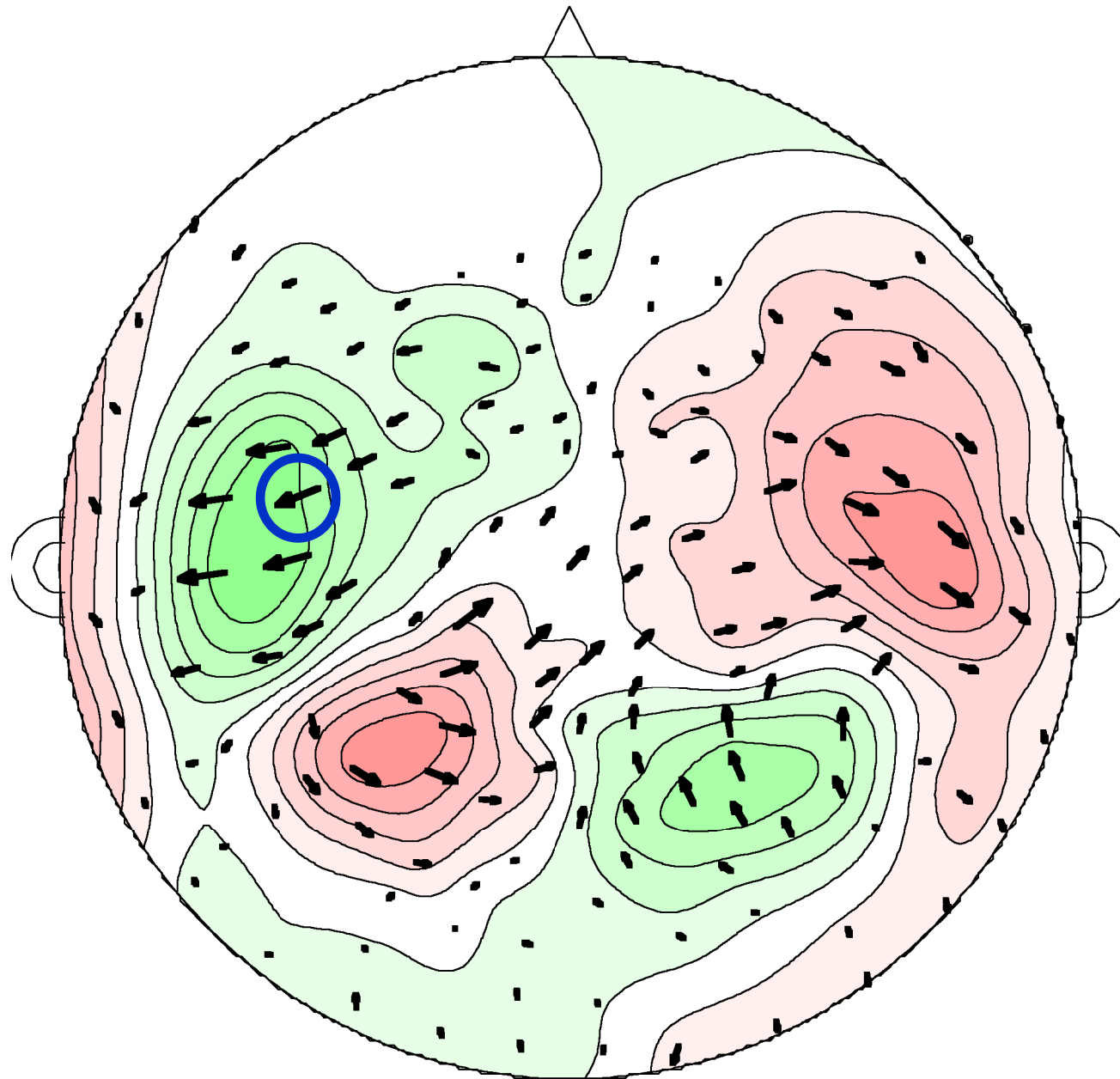
32 Hz Modulation
400 Hz tone carrier
100 trials @ 1 s
(concatenated)



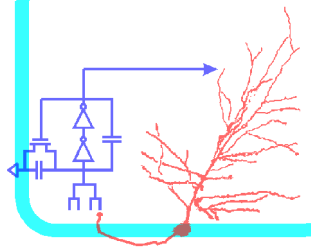
Extremely Precise Phase-Locking: 0.01 Hz
No trial-to-trial jitter



Whole-Head SSR

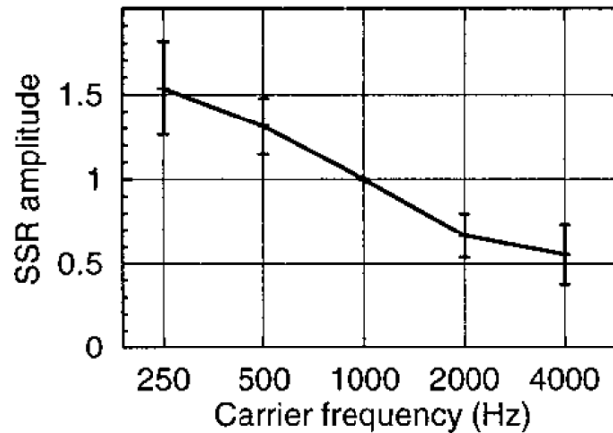


32 Hz

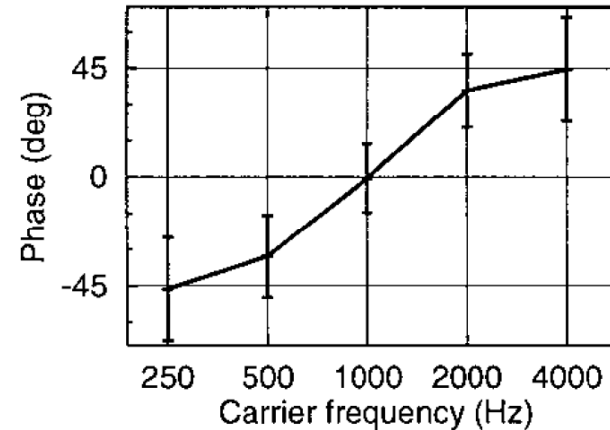


SSR Carrier Dependence

SSR Amplitude

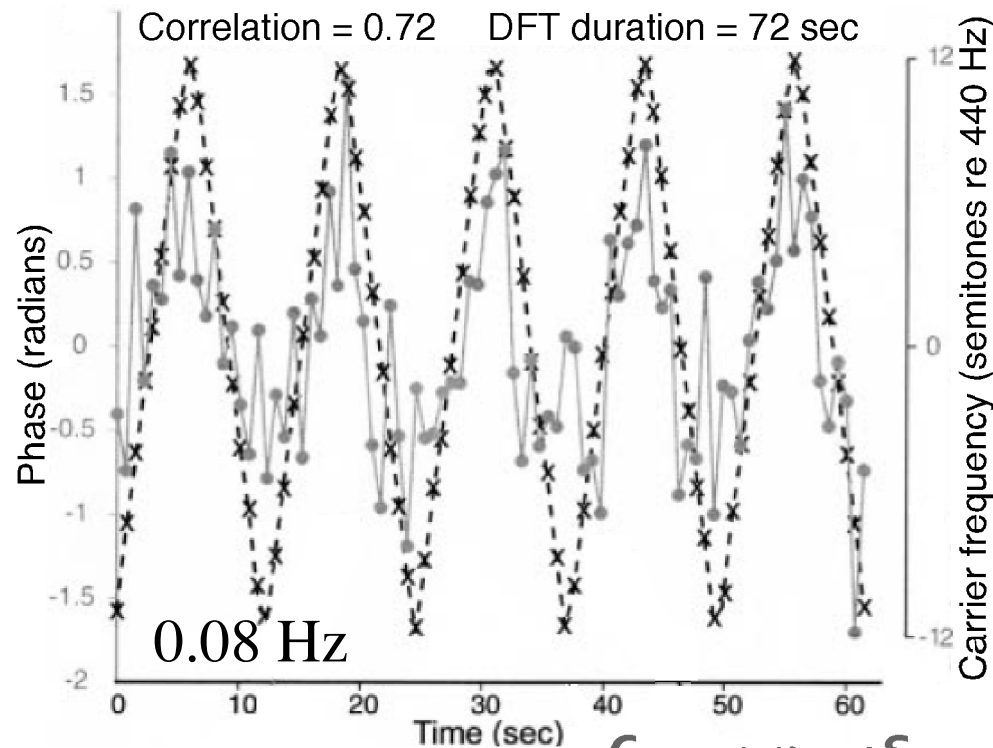


SSR Phase

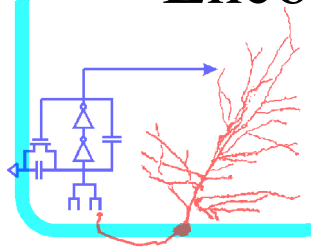


*Ross et al.
(2000)*

SSR Phase
Follows
Carrier
↓
Phase
Modulation
Encoding



*Patel &
Balaban
(2004)*



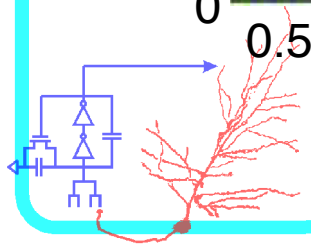
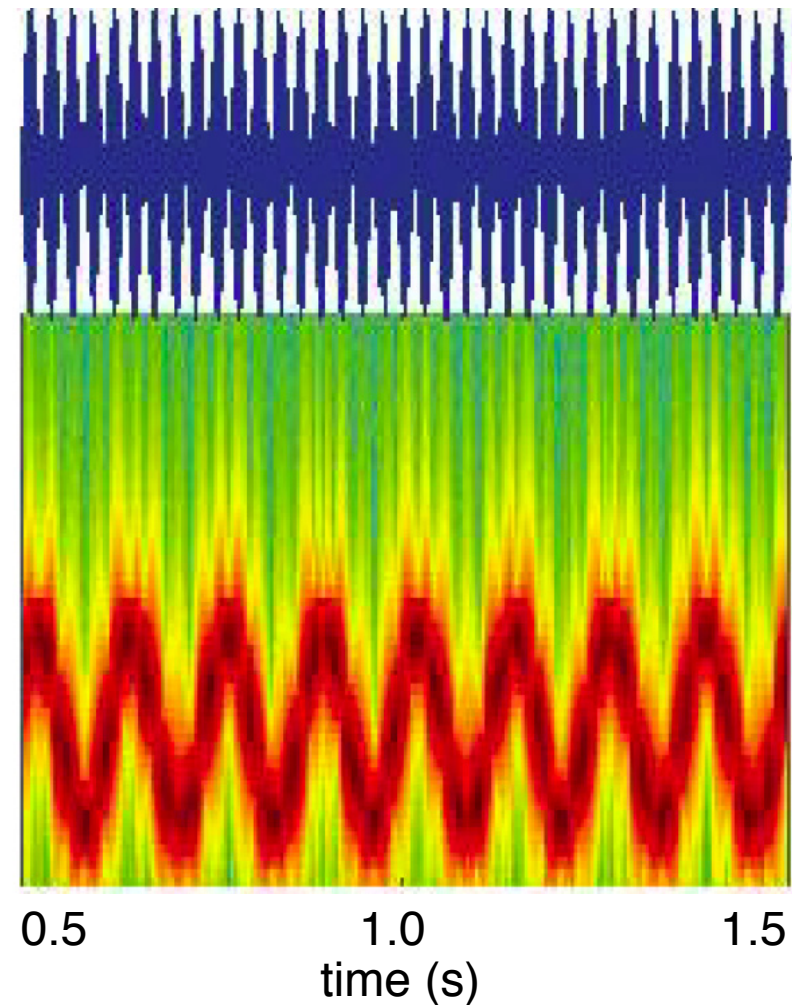
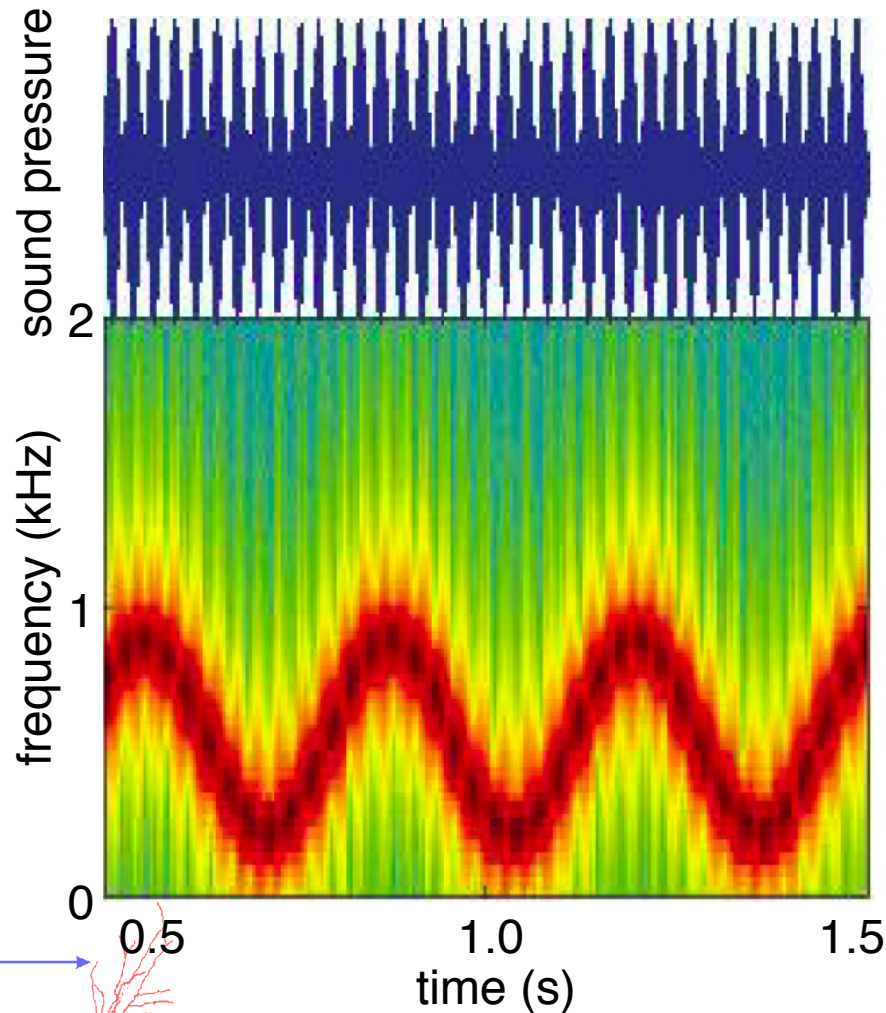
Sample Dual Modulation Stimuli

$$f_{\text{FM}} = 3.1 \text{ Hz}$$

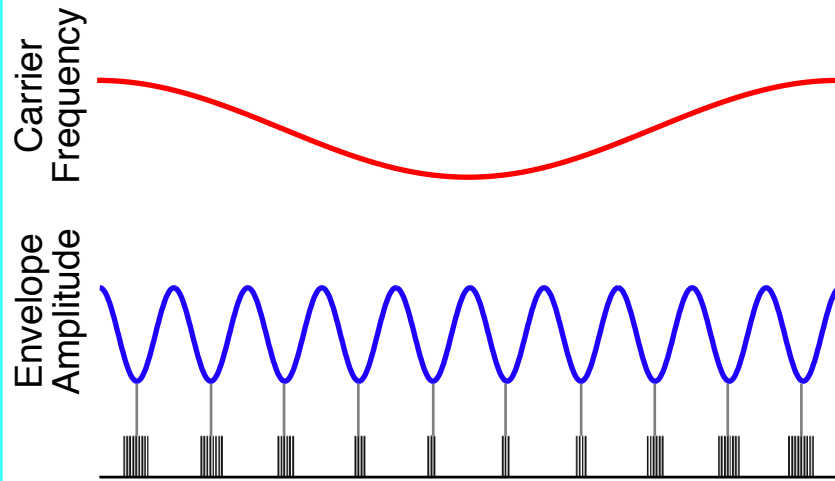
$$f_{\text{AM}} = 37 \text{ Hz}$$

$$f_{\text{FM}} = 8 \text{ Hz}$$

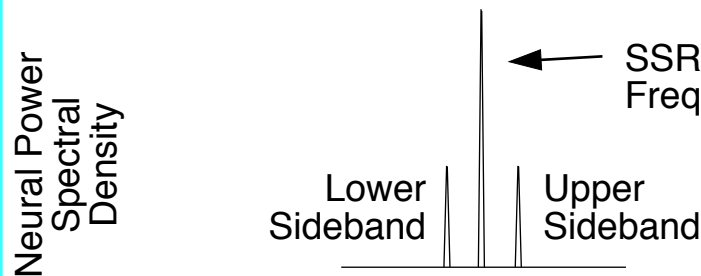
$$f_{\text{AM}} = 37 \text{ Hz}$$



Neural Modulation Models



Amplitude Modulation
(AM)
Coding

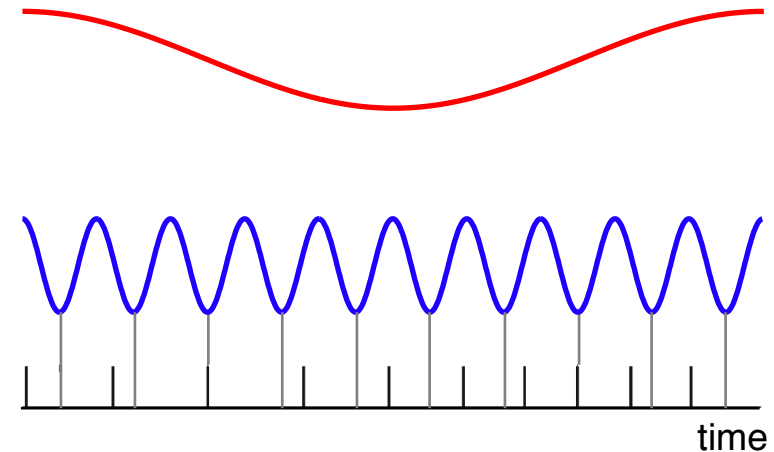


Neural Response Spectrum

Stimulus
Carrier
Frequency
(FM)

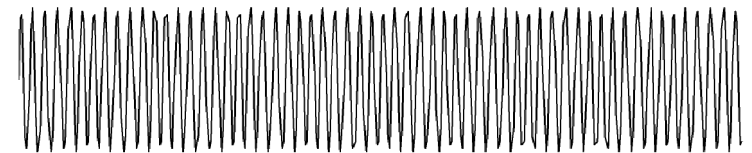
Stimulus
Envelope
Amplitude
(AM)

Neural
Modulation
Coding



Phase Modulation
(PM)
coding

Neural
Averaged
Response



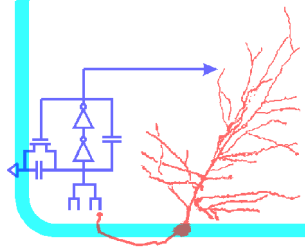
c.f.
Patel &
Balaban
(2004)

$$\alpha = (\varphi_{upper} - \varphi_{SSR}) - (\varphi_{SSR} - \varphi_{lower})$$

Neural Response
Phase Encoding
Parameter

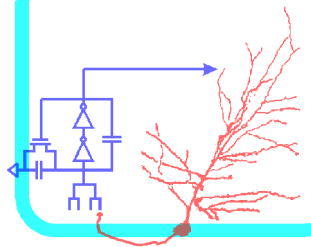
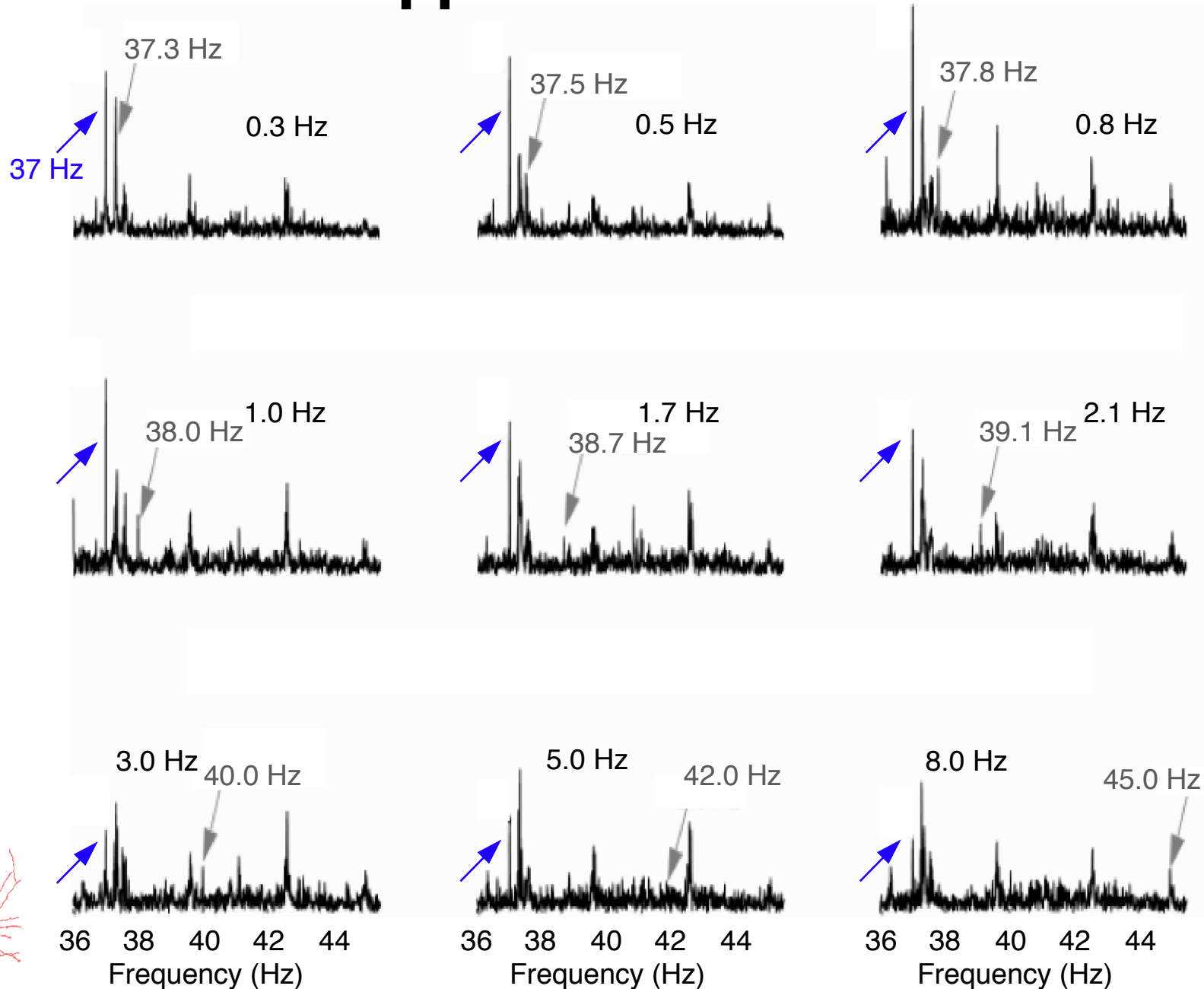
$$\alpha_{AM} = 0 \text{ or } 2\pi$$

$$\alpha_{PM} = \pi$$



Spectral Sideband Responses

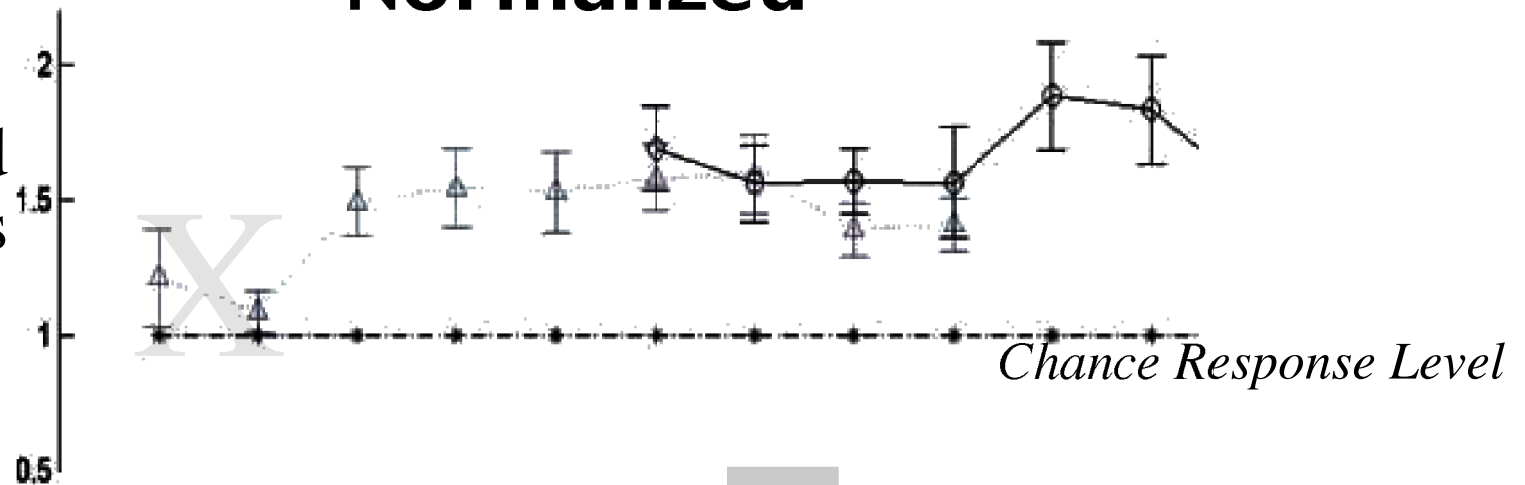
upper sidebands



Sideband Responses

Normalized

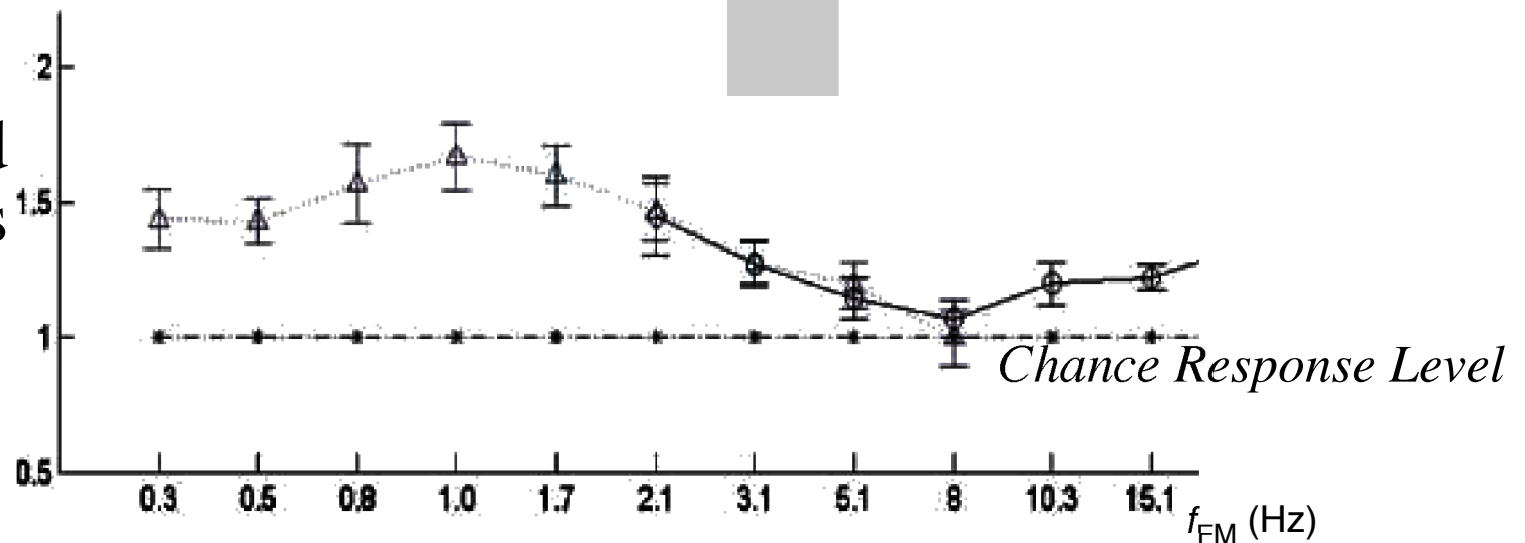
Upper Sideband Responses



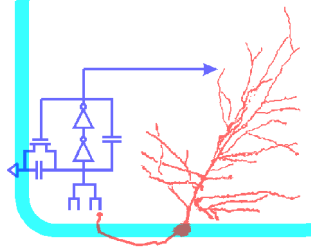
Both Sidebands contribute

Only Upper Sideband contributes

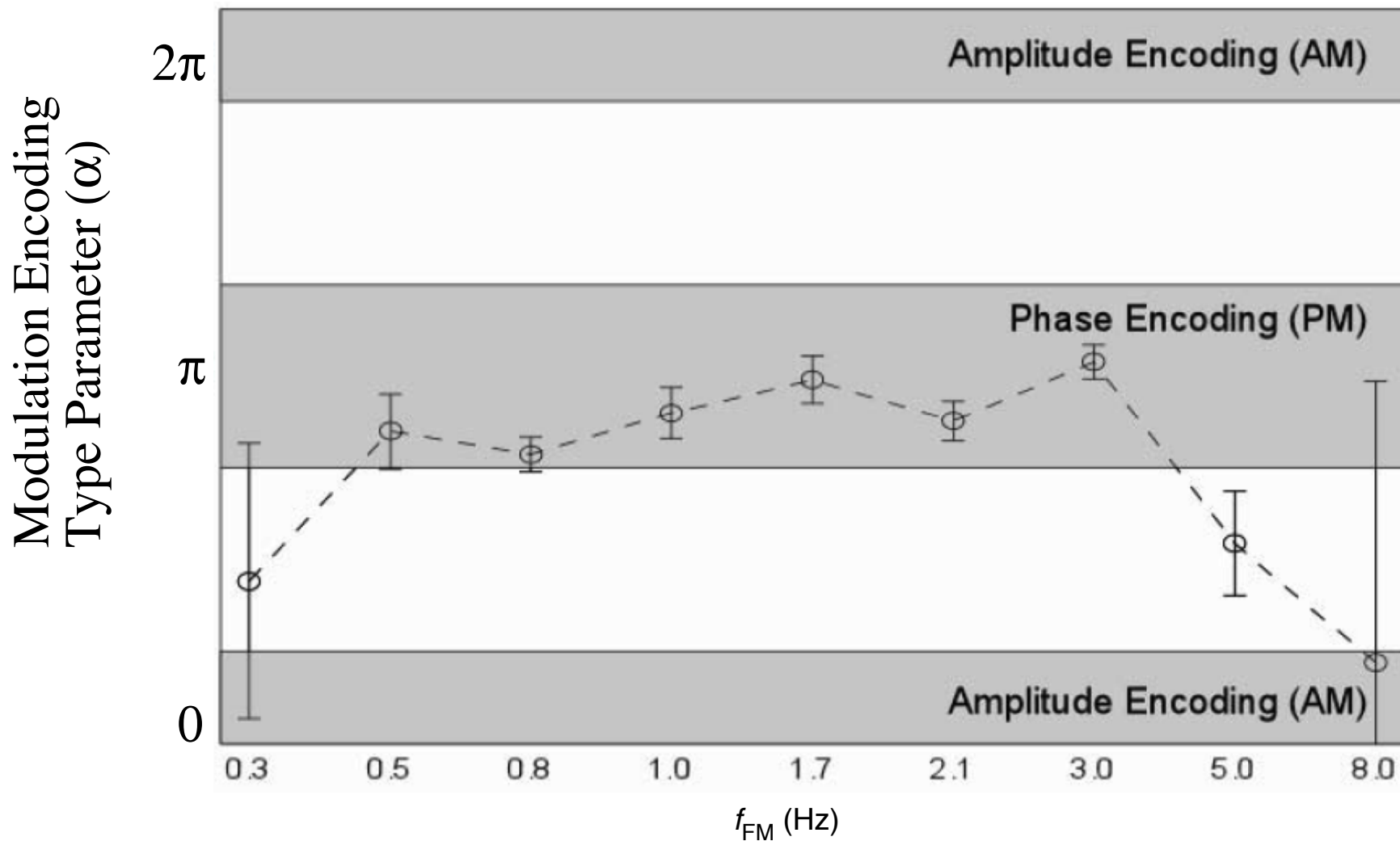
Lower Sideband Responses



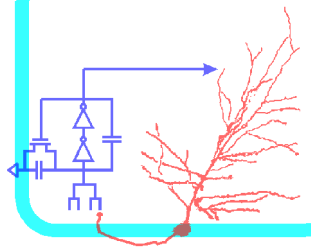
Modulation Encoding, with coding transition at $f_{FM} \sim 5$ Hz



Modulation Encoding Type



Phase Modulation Encoding below $f_{FM} \sim 5$ Hz



Conclusions

- MEG can address questions of Neural Coding
 - Coarseness of Localization not Intrinsic Obstacle
 - Modulation encoding gives family of response types
- Combined AM/FM modulations are encoded in Auditory Cortex
 - Phase Modulation seen at lowest FM rates
 - Modulation Encoding changes at higher rates
- Single Sideband Modulation unexpected
 - Speculate: Single Modulation Encoding type?
 - Or: Two populations of AM and PM encoding neurons whose phase happens to cancel in lower sideband?

